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# NEURORADIOLOGY

ORIGINAL ARTICLE

Do the combination of multiparametric MRI-based radiomics and selected blood inflammatory markers predict the grade and proliferation in glioma patients?

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Received 10 April 2020; revision requested 8 May 2020; last revision received 24 August 2020; accepted 29 August 2020.

Published online 24 March 2021.

DOI 10.5152/dir.2021.20154

#### PURPOSE

We aimed to explore whether multiparametric magnetic resonance imaging (MRI)-based radiomics combined with selected blood inflammatory markers could effectively predict the grade and proliferation in glioma patients.

## METHODS

This retrospective study included 152 patients histopathologically diagnosed with glioma. Stratified sampling was used to divide all patients into a training cohort (n=107) and a validation cohort (n=45) according to a ratio of 7:3, and five-fold repeat cross-validation was adopted in the training cohort. Multiparametric MRI and clinical parameters, including age, the neutrophil-lymphocyte ratio and red cell distribution width, were assessed. During image processing, image registration and gray normalization were conducted. A radiomics analysis was performed by extracting 1584 multiparametric MRI-based features, and the least absolute shrinkage and selection operator (LASSO) was applied to generate a radiomics signature for predicting grade and Ki-67 index in both training and validation cohorts. Statistical analysis included analysis of variance, Pearson correlation, intraclass correlation coefficient, multivariate logistic regression, Hosmer–Lemeshow test, and receiver operating characteristic (ROC) curve.

### RESULTS

The radiomics signature demonstrated good performance in both the training and validation cohorts, with areas under the ROC curve (AUCs) of 0.92, 0.91, and 0.94 and 0.94, 0.75, and 0.82 for differentiating between low and high grade gliomas, grade III and grade IV gliomas, and low Ki-67 and high Ki-67, respectively, and was better than the clinical model; the AUCs of the combined model were 0.93, 0.91, and 0.95 and 0.94, 0.76, and 0.80, respectively.

### CONCLUSION

Both the radiomics signature and combined model showed high diagnostic efficacy and outperformed the clinical model. The clinical factors did not provide additional improvement in the prediction of the grade and proliferation index in glioma patients, but the stability was improved.

G lioma is the most common primary malignant tumor in the brain, accounting for nearly 81% of malignant tumors in the brain (1). In the 2016 World Health Organization (WHO) classification system, gliomas can be graded from level I to level IV according to the histopathological and clinical criteria. Low-grade gliomas (LGGs) include grades I and II, whereas high-grade gliomas (HGGs) include grades III and IV (2, 3). Patients with LGGs may remain indolent for years or progress to glioblastoma (4) and are generally treated with only surgery and in some cases with radiotherapy (5). For patients with HGGs, radiotherapy and/or chemotherapy are usually followed after surgery, which often indicates a poor prognosis (6). Although genetic factors play an increasingly important role in indicating prognosis and survival (2, 3, 7), false classification could directly cause inappropriate treatment, which significantly affects patient outcomes. Hence, precise grading is still crucial for therapy planning and progression assessment in patients with gliomas.

The nuclear protein Ki-67 is a reliable biomarker for evaluating the proliferation of tumor cells, because it only exists in active phase of the cell cycle. (8). The Ki-67 labeling index (LI) is defined as the percentage of Ki-67-positive tumor nuclei of all tumor nuclei (9). The WHO reported that the Ki-67 LI values are below 4% of the mean value for grade II glioma, 5%–10%

You may cite this article as: Guo J, Ren J, Cheng R, He Y, Shen J. Do the combination of multiparametric MRI-based radiomics and selected blood inflammatory markers predict the grade and proliferation in glioma patients? Diagn Interv Radiol 2021; 27:440–449

for grade III glioma, and 15%–20% for grade IV glioma (2). The overexpression of Ki-67 infers poor differentiation and prognosis (10). Hence, the accurate preoperative evaluation of the Ki-67 LI maybe helpful in treatment decision-making for glioma patients.

Recently, there is a newly emerging area in radiology: radiomics, which is realized by quantifying image data with advanced image post-processing techniques (11). For tumor radiomics, a complete characterization of the tumor is established by feature selection and high-throughput analysis (12, 13). The radiomics analysis of glioma MRI could predict the grade and proliferation potency in glioma patients (14-16). A study showed that multiparametric MRI-based radiomics analysis, assisted by T2-weighted imaging, gadolinium-based contrast-enhanced T1-weighted imaging and the apparent diffusion coefficient (ADC), could help clinicians classify gliomas more accurately (17).

Chronic inflammation, which is part of the tumor microenvironment, is associated with tumor occurrence and progression (18, 19). Some blood inflammatory biomarkers, such as the neutrophil-lymphocyte ratio (NLR), platelet count, and red cell distribution width (RDW), have been proposed to predict the prognosis of tumors (20–22). And recent studies showed that the NLR and platelet count in glioblastoma patients (23, 24) and the NLR and RDW in glioma patients were significant in predicting prognosis (25).

## **Main points**

- The clinical model included age, neutrophil-lymphocyte ratio and red cell distribution width.
- Radiomics analysis is based on multiparametric MRI, including T2-weighted, T1-weighted, T2 FLAIR and contrast-enhanced T1-weighted imaging.
- Among the radiomics features, factors related to heterogeneities in T2 FLAIR and contrast-enhanced T1-weighted imaging were the most important components for predicting between LGGs and HGGs, grade III and grade IV, and low Ki-67 and high Ki-67.
- Radiomics was better for differentiating LGGs and HGGs, grade III and grade IV gliomas, and low Ki-67 and high Ki-67 than the clinical model.
- The combination of radiomics and the clinical model could improve the predictive stability of the grade and proliferation in glioma patients.

To our knowledge, there have been no studies on MRI-based radiomics combined with selected blood inflammatory markers to predict the grade and proliferation potency in glioma patients. The purpose of this study is to build and assess a radiomics nomogram to preoperatively predict glioma grade and proliferation potency by incorporating MRI-based radiomics and clinical signatures, including age, NLR, and RDW.

# Methods

The radiological and surgical databases were retrospectively reviewed for records from 2013 to 2018. This study was approved by our institutional ethics committee and the requirement for informed consent was waived due to retrospective analysis (202001). The inclusion criteria for patients were: (a) Histopathologically confirmed supratentorial glioma except grade I; (b) Preoperative craniocerebral MRI including T2- and T1-weighted imaging, T2-weighted attenuated inversion recovery imaging (T2 FLAIR) and contrast-enhanced T1-weighted imaging; and (c) patients with Ki-67 LI values. Nineteen of these patients were excluded because of: treatment (chemoradiotherapy, chemotherapy or radiotherapy) prior to the MRI examination (n=10); and poor imaging guality rendering the image unqualified for image analysis due to the influence of motion or susceptibility (n=9). Finally, this study included 152 patients (47, 39 and 66 patients were diagnosed as grade II, III and IV gliomas, respectively). In our study, the low expression level of Ki-67 was defined as  $\leq 10\%$  positive staining (n=56), whereas the high expression level of Ki-67 was defined as >10% positive staining (n=96) (26). Stratified sampling was used to divide all patients into a training cohort (n=107) and a validation cohort (n=45) according to a ratio of 7:3.

#### **MRI protocol**

All included patients were examined with a 3.0 Tesla MRI scanner (Trio, Siemens). Axial T2-weighted imaging, T2 FLAIR, unenhanced and contrast-enhanced T1-weighted imaging were performed. The acquisition parameters were as follows: T2-weighted imaging: slice thickness, 4.5 mm; intersection gap, 4.5 mm; repetition time (TR)/echo time (TE), 7140/98 ms; field of view (FOV), 22×22 cm<sup>2</sup>; pixel matrix, 384×384; acquisition time, 2 min 17 s; flip angle, 150°; T2 FLAIR: slice thickness, 4.5 mm; intersection gap, 0.45 mm; TR/TE, 8400/91 ms; FOV, 24×24 cm<sup>2</sup>; pixel matrix, 256×256; acquisition time, 2 min 16 s; flip angle, 130°; and T1-weighted imaging: slice thickness, 4.5 mm; intersection gap, 0.45 mm; TR/TE, 220/3 ms; FOV, 22×22 cm<sup>2</sup>; pixel matrix, 256×256; acquisition time, 44 s; flip angle, 70°. A dosage of 0.2 mL/kg gadopentetate dimeglumine was given intravenously and axial contrast-enhanced T1-weighted imaging was acquired.

### Volume-of-interest (VOI) segmentation

The T2 FLAIR, unenhanced and contrast-enhanced T1-weighted imaging were co-registered with reference to the T2-weighted imaging using Slicer (version: 4.10.1, package: Elastix, https://www.slicer. org). The tumor VOIs covered the most representative regions of the gliomas by manual segmentation in the T2-weighted imaging using the ITK-SNAP software (version: 3.8.0, https://www.itksnap.org). For the VOI delineation, the tumor boundaries of nonenhancing gliomas were determined in T2-weighted imaging, because in these tumors hyperintense signals represented the tumor regions of gliomas; meanwhile, for the enhancing gliomas the most representative regions were decided in T2-weighted imaging with reference to the contrast-enhanced T1-weighted imaging to separate the parenchymal areas from edematous areas and avoid the inclusion of obvious cysts, necrosis and hemorrhage regions. Then, the contours of the VOIs on the T2-weighted imaging were copied to images of other MRI sequences. The segmentation of the VOIs was performed independently by a senior neuroradiologist. To verify the consistency between readers, the VOIs of 30 randomly selected cases were segmented by another senior neuroradiologist. The segmentation of the VOIs is presented in Fig. 1.

# Radiomics features extraction and radiomics signature construction

All MRI data underwent image resampling to isotropic voxels  $(1 \times 1 \times 1 \text{ mm})$  with linear interpolate, and intensity normalization (Z-score) before feature extraction (27) and radiomics features were calculated by Artificial Intelligence Kit (AK, version: 3.2.1, GE Healthcare). Overall, 396 radiomics features were extracted from each sequence for each patient, including 42 histogram features, 9 form factor features, 144 gray level cooccurrence matrix (GLCM) features, 180 run-length matrix (RLM) features, 11



gray level size zone matrix (GLSZM) features and 10 Haralick features.

The interobserver intraclass correlation coefficient (ICC) selects values greater than 0.75, and T2 FLAIR, unenhanced and contrast-enhanced T1-weighted imaging and T2-weighted imaging had 346, 358, 357, and 243 features reserved, respectively. The results indicated favorable interobserver feature extraction reproducibility. Before feature selection, all the radiomics features were standardized by the Z-score method.

Then, feature selection was conducted as follows: First, analysis of variance (ANOVA) was performed to remove features with p > 0.05, followed by the correlation test to remove features that had a correlation coefficient > 0.9. Next, the least absolute shrinkage and selection operator (LASSO) model, which could improve prediction accuracy and interpretation (28, 29), was used to further select the features. The reserved features were applied to construct the radiomics score for every patient.

# Assessment of the radiomics score, clinical model and radiomics nomogram

The radiomics score, which was derived from individual sequences and multiparametric MRI, and significant clinical data (age, NLR, and RDW) (23–26) were used as potential predictors for the multivariate logistic regression analysis to build a prediction model of the grade and proliferation potency of gliomas. The radiomics nomogram was also constructed by combining the radiomics score derived from multiparametric MRI and

Table 1. Characteristics of the patients in the training and validation cohorts								
		Tra	aining cohort (n=107	)	Validation cohort (n=45)			
		Grade II	Grade III	Grade IV	Grade II	Grade III	Grade IV	
n		36	28	43	11	11	23	
Age (years), mean±SD		44.38±11.31	48.04±12.02	54.46±12.58	40.18±8.85	56.73±10.98	56.83±13.07	
NLR, median (Q1, Q3)		2.07 (1.72, 3.22)	2.44 (1.84, 3.51)	2.83 (2.07, 5.14)	1.83 (1.48, 2.9)	3.42 (2.56, 4.4)	3.00 (2.30, 5.4)	
RDW, mean±SD		13.1±1.04	13.34±1.05	13.37±1.52	13.21±1.38	12.87±0.58	13.42±0.86	
Ki-67 Ll, n	≤10%		42			14		
	>10%		65			31		

SD, standard deviation; NLR, neutrophil-lymphocyte ratio; Q1–Q3, 25<sup>th</sup> and 75<sup>th</sup> percentiles; RDW, red cell distribution width; Ki-67 Ll, Ki-67 labeling index.



**Figure 2.** Flowchart of constructing a radiomic nomogram with multiparametric MRI and clinical features to predict the glioma grade and proliferation potency. T2WI, T2-weighted imaging; CE T1WI, contrast-enhanced T1-weighted imaging; NLR, neutrophil-lymphocyte ratio; RDW, red cell distribution width.

clinical factors. The performance of the radiomics score, clinical model and radiomics nomogram was evaluated by using a calibration curve. The radiomics score, clinical model and radiomics nomogram were applied in the validation cohort subsequently by using the same formula in the training cohort. Additionally, the no-information rate was calculated in our dataset for comparison with the diagnosis accuracy. A simplified flowchart of the study is given in Fig. 2.

## **Statistical analysis**

The LASSO method was utilized in conjunction with the penalty parameter adjustment and is performed through five-fold repeat cross-validation based on the minimum deviation criteria. Backward stepwise selection was utilized by dint of the likelihood ratio test, and Akaike's information criterion (AIC) was taken as the stopping rule for the multivariate logistic regression.

The accuracy of the radiomics score was quantified by the area under the receiver operating characteristic (ROC) curve (AUC) in both the training and validation cohorts. The range of 95% confidence interval was used to evaluate the stability of the models. The Hosmer–Lemeshow test were used to assess the goodness-of-fit and discriminatory ability. ICCs were used to evaluate the interobserver agreement.

All the statistical analyses were conducted with R software (version 3.5.3; https://ww-

w.r-project.org). The "rms" package was used to construct the nomogram. All the reported statistical significance levels were two-sided, with statistical significance of 0.05.

# Results

There were no significant differences in age, NLR, RDW, glioma grading, and Ki-67 expression (p > 0.05) between the training and validation cohorts. There were statistically significant differences in age and NLR variables among LGGs and HGGs. The characteristics of all the participants are shown in Table 1 and Supplementary Tables 1–3.

The results of the data dimension reduction with LASSO are shown in Fig. 3a, 3c, 3e. LASSO with 11, 9, and 12 of the most important variables and their coefficients are shown in Fig. 3b, 3d, 3f, which indicate great diagnostic potential. All the reserved features and the best-performing features are listed in Table 2. The logistic regression models predicted the grade and proliferation potency of gliomas as shown in the following formulas:

Grade = 1.978 + 0.855 \* flair\_InverseDifferenceMoment\_angle45\_offset7 + 0.8286 \* t2\_skewness -0.550 \* t1c\_kurtosis -1.061 \* t1c\_uniformity -+ 1.925 \* t1c\_Inertia\_angle90\_offset1

Grade34 =0.9185 + 1.8657\*t1\_skewness + 1.3046 \* t2\_Range + 2.3632 \* t1c\_Inertia\_angle90\_offset1 - 0.9154 \* t1c\_LowIntensitySmallAreaEmphasis

Ki67 = 1.263 + 1.326 \* flair\_Correlation\_angle0\_offset7 + 0.898 \* t1\_LongRunEmphasis\_angle45\_offset1 + 0.673 \* t2\_skewness -0.713 \* t2\_ShortRunHigh-GreyLevelEmphasis\_AllDirection\_offset4\_SD - 0.888 \* t1c\_kurtosis + 1.346 \* t1c\_Inertia\_angle90\_offset1 - 0.917 \* t1c\_ LargeAreaEmphasis

The AUCs of the radiomics score derived from multiparametric MRI were signifi-



**Figure 3. a**–**f.** Feature selection using LASSO. The tuning parameter ( $\lambda$ ) selection in the LASSO model used ten-fold cross-validation with minimum criteria and could predict low-grade gliomas (LGGs) and high-grade gliomas (HGGs) (**a**), grade III and grade IV gliomas (**c**), and low Ki-67 and high Ki-67 (**e**). LASSO coefficient profiles of texture features could predict LGGs and HGGs (**b**), grade III and grade IV gliomas (**d**), and low Ki-67 and high Ki-67 (**f**).



Figure 4. a-c. The ROC curves show the effectiveness of combining the radiomics score and clinical factors in differentiating between LGGs and HGGs (a), grade III and grade IV gliomas (b), and low Ki-67 and high Ki-67 (c) in the training cohort.

cantly higher than those of the models of individual sequences in differentiating between LGGs and HGGs, grade III and grade IV glioma, and low Ki-67 and high Ki-67 in the training and validation cohorts (Supplementary Fig.). The radiomics score derived from multiparametric MRI was significantly correlated with glioma grading and Ki-67 expression (p < 0.001). In the training cohort, the AUCs of the radiomics score for differentiating between LGGs and HGGs, grade III and grade IV glioma, and low Ki-67 and high Ki-67 were 0.92, 0.91 and 0.94, respectively, which were significantly higher

than those of clinical factors, and the De Long test p values were all < 0.001. After combining the radiomics score and clinical factors, the AUCs were 0.93, 0.91 and 0.95, respectively (Fig. 4), and all of the De Long test p values were < 0.001 compared with clinical factors. These results suggested that the performance was best when multiparametric MRI and clinical factors were considered simultaneously. The calibration curve of radiomics nomogram also showed that the predicted probability was in good agreement with actual

Table 2. Radiomic feature selection results								
	T2WI	T1WI	T2 FLAIR	CET1WI				
LGGs and HGGs	1		1	3				
	Skewness		Inverse Difference- Moment_angle45_ offset7	Kurtosis				
				Inertia_angle90_ offset1 uniformity				
Grade III and IV	2	1		5				
	Percentile95	MinIntensity		kurtosis				
	Range			SmallAreaEmphasis				
				LowIntensity SmallAreaEmphasis				
				Variance				
				Inertia_angle90_ offset1				
Low Ki-67 Ll and high Ki-67 Ll	2	1	1	3				
	Skewness	t1_LongRunEm- phasis_angle45_ offset1	flair_Correlation_ angle0_offset7	t1c_kurtosis				
	ShortRunHigh- GreyLevelEm- phasis_AllDirec- tion_offset4_SD			Inertia_angle90_off- set1				
				t1c_LargeAreaEm- phasis				
T2WI, T2-weighted imaging; T1WI, T1-weighted imaging; T2 FLAIR, T2-weighted attenuated inversion recovery								

probability in the training cohort (Fig. 5). The predictive performances of the radiomics score, clinical factors and their combination are shown in Fig. 6. The Hosmer–Lemeshow test demonstrated no significant differences (p = 1.00, p = 0.39, and p = 0.24) and indicated no deviation from a perfect fit.

In the validation cohort, the findings were similar. The radiomics score and combination strategy showed favorable performances. The Hosmer-Lemeshow test indicated no significant difference (p = 1.00) in differentiating between LGGs and HGGs, but significant differences in differentiating between grade III and grade IV gliomas (p = 0.002) and low Ki-67 and high Ki-67 (p = 0.002). The diagnostic performance of the three proposed models is shown in Table 3. Additionally, for the measure of class imbalance, the no-information rates between LGGs and HGGs, grade III and grade IV glioma, and low and high Ki-67 were 0.6216, 0.621 and 0.6075 in the training cohort and 0.645, 0.645 and 0.689 in the validation cohort, respectively. The radiomics and nomogram model prediction accuracy all exceeded the no-information rate.

# Discussion

This study predicted the grade and proliferation potency in glioma patients by developing a radiomics nomogram. The model combined multiparametric MRI-based radiomics and clinical factors, including age and selected blood inflammatory markers, and showed good discriminative ability.

12WI, 12-weighted imaging; 11WI, 11-weighted imaging; 12 FLAIR, 12-weighted attenuated inversion recovery imaging; CE T1WI, contrast-enhanced T1-weighted imaging; LGGs, low-grade gliomas; HGGs, high-grade gliomas; Ki-67 LI, Ki-67 labeling index.

## Table 3. Diagnostic performance of the three proposed models

		Training cohort				Validation cohort			
Different models		Sensitivity	Specificity	Accuracy	AUC (95% CI)	Sensitivity	Specificity	Accuracy	AUC (95% CI)
Clinical	LGGs and HGGs	0.80	0.52	0.62	0.70 (0.59–0.80)	0.64	0.97	0.89	0.82 (0.66–0.99)
	Grade III and Grade IV	0.82	0.57	0.66	0.65 (0.51–0.78)	1.00	0.30	0.55	0.60 (0.39–0.80)
	Low Ki-67 LI and High Ki-67 LI	0.45	0.82	0.67	0.67 (0.56–0.77)	0.43	1.00	0.82	0.72 (0.54–0.90)
Radiomics	LGGs and HGGs	0.94	0.85	0.88	0.92 (0.87–0.97)	1.00	0.82	0.87	0.94 (0.87–1.00)
	Grade III and Grade IV	0.86	0.89	0.88	0.91 (0.83–0.99)	0.82	0.60	0.68	0.75 (0.57–0.93)
	Low Ki-67 LI and High Ki-67 LI	0.93	0.83	0.87	0.94 (0.89–0.98)	0.64	0.94	0.84	0.82 (0.69–0.96)
Combined	LGGs and HGGs	0.92	0.85	0.87	0.93 (0.89–0.98)	1.00	0.88	0.91	0.94 (0.87–1.00)
	Grade III and Grade IV	0.79	0.96	0.89	0.91 (0.83–0.99)	0.73	0.70	0.80	0.76 (0.58–0.94)
	Low Ki-67 LI and High Ki-67 LI	0.91	0.88	0.89	0.95 (0.91–0.99)	0.86	0.68	0.73	0.80 (0.66–0.94)

AUC, area under the curve; 95% CI, 95% confidence interval; LGGs, low-grade gliomas; HGGs, high-grade gliomas; Ki-67 LI, Ki-67 labeling index.



Figure 5. a-c. Calibration of the radiomics nomogram to predict LGGs and HGGs (a), grade III and grade IV gliomas (b), and low Ki-67 and high Ki-67 (c) in the training cohort.

The conventional presurgical determination of glioma grades mainly depends on conventional MRI techniques, including T2- and T1-weighted imaging, T2 FLAIR and, particularly, contrast-enhanced T1-weighted imaging. However, conventional MRI provides limited information regarding glioma grading, and the accuracy is only 55% to 83%. A study showed that 20% of LGGs show contrast enhancement, whereas a third of HGGs do not show contrast enhancement (30). In addition, conventional MRI is unable to evaluate tumor proliferation potency. A few studies have used advanced MRI sequences, such as multi-b-value diffusion-weighted imaging, diffusion tensor imaging (DTI), diffusion kurtosis imaging (DKI), and dynamic contrast-enhanced perfusion imaging (DCE-MRI), for the grading or proliferation potency evaluation of gliomas (31–37). Ren et al. (31) showed that the heterogeneity index  $\alpha$ and slow diffusion coefficient derived from non-Gaussian diffusion MRI could improve the accuracy of glioma grading and predict the proliferation level of malignant gliomas. Mean diffusivity derived from DTI could also be used in grading gliomas, and the ROC curve showed a sensitivity of 91.8% (32). It has also been reported that DKI is superior to DTI in predicting the grade and proliferation potency, and average kurtosis is suggested to be the best prediction parameter (33-36). Jain et al. (37) demonstrated some potential advanced MRI parameters for differentiating LGGs and HGGs. The sensitivity and specificity of the relative cerebral blood volume (rCBV) in differentiating LGGs and HGGs were 97.22% and 100%, respectively. Additionally, rCBV, volume transfer constant (Ktrans) and volume of extravascular extracellular space per unit volume of tissue ( $V_e$ ) were associated with the Ki-67 Ll in HGGs (38). Data analysis based on advanced imaging has gained increasing attention; however, the time-consuming processes and some uncertain results limit its fast popularization.

The radiomics score was an independent predictor of the grade and proliferation potency in glioma patients (39). Wang et al. (17) extracted features from T2-weighted imaging, ADC and contrast-enhanced T1-weighted imaging sequences. They compared the radiomic features of HGGs with that of LGGs. Their results showed 15 features with significant differences between HGGs and LGGs, and the diagnostic efficiency could be improved by combining these 15 features (with AUCs of 0.971 and 0.961 in the training and validation cohorts, respectively). This approach indicates that multiparametric MRI-based radiomic features play an important role in glioma grading. Cho et al. (40) combined T2-weighted imaging, T1-weighted imaging, T2 FLAIR and contrast-enhanced T1-weighted imaging and used machine learning, feature selection techniques and a radiomics approach for glioma grading. They extracted 5 significant features that showed an average AUC of 0.9400 for the training cohort and 0.9030 for the validation cohort.

In our study, we performed a radiomics analysis based on individual sequences and multiparametric MRI, including T2-weighted imaging, T1-weighted imaging, T2 FLAIR and contrast-enhanced T1-weighted imaging. The results showed that the radiomics score derived from multiparametric MRI was superior to that of the models of individual sequences, and in the former the results

showed that the selected radiomics features related to heterogeneities in T2 FLAIR and contrast-enhanced T1-weighted imaging were the most important components in differentiating LGGs and HGGs, grade III and grade IV, and low and high Ki-67. The reason might be because T2 FLAIR could provide more information on edema, and contrast-enhanced T1-weighted imaging contains more information about blood supply, necrosis and blood-brain barrier damage due to gliomas, which are related with the grading and Ki-67 LI of gliomas. Skewness, kurtosis, range, variance, uniformity and percentil95 are first order features used to describe the degree of uniform distribution of signal strength in tumors. Inertia, InverseDifferenceMoment, ClusterProm-ShortRunHighGrayLevelEmphasis inence, and LongRunEmphasis are texture features that mainly describe the heterogeneity within the tumor, and the heterogeneity within malignant tumors is higher. The AUCs of the radiomics score were 0.92 and 0.94 in the training cohort and validation cohort for differentiating LGGs and HGGs, respectively, which is consistent with that of a previous study (14). In addition, grade III and grade IV gliomas could be well differentiated by the extracted variables with LASSO, and the AUC was 0.91 and 0.75 in the training cohort and validation cohort, which is lower than that for the differentiation of LGGs and HGGs. However, the performance is of value in differentiating grade III and grade IV gliomas. Due to the differences of prognosis and treatment between grade III and grade IV gliomas, their classification is essential. Even though only a few studies have focused on differentiating grade III and grade IV gliomas, our results were consistent with



those of previous studies (AUCs of 0.881 and 0.992) (16, 39). However, those studies were limited by the lack of an independent validation cohort.

A previous study investigated the radiomic features related to the Ki-67 LI in gliomas for tumor proliferation prediction. The results showed that the radiomics signature based on T2-weighted imaging could predict Ki-67 LI in LGGs, with accuracies of 83.3% and 88.6% (AUCs of 0.91 and 0.93) in the training and validation cohorts, respectively (40). Su et al. (16) explored the diagnostic performance of radiomics based on multiparametric MRI, including T1- and T2-weighted imaging, T2 FLAIR, contrast-enhanced T1-weighted imaging, ADC and arterial spin labeling, for predicting tumor proliferation and found that the AUC was 0.936, which is consistent with our results (AUCs of 0.94 and 0.82 in the training and validation cohort, respectively). Hence, multiparametric MRI-based radiomics could be used to predict the proliferation potency of gliomas.

Chronic inflammation is characteristic of tumor microenvironment, stimulating tumor progression and metastasis. Some studies have suggested that peripheral inflammatory states, such as the NLR, platelet count and RDW, could predict prognosis in patients with glioma (23, 24). Auezova et al. (25) assessed the association of the NLR, platelet count and RDW with tumor grade and survival in glioma patients and found that only the NLR and RDW was helpful to assess progression and outcomes. Weng et al. (41) suggested that the combination of radiologic biomarkers (including contrast enhancement) and peripheral parameters such as the NLR could successfully predict proliferation potency in glioma patients. They found that there were significant correlations between the NLR and tumor grade or proliferation potency and between the platelet count and tumor grade or proliferation potency, whereas no correlation existed between the monocyte-lymphocyte ratio (MLR) and grade or proliferation potency. However, they assessed the value of features from only conventional MRI such as contrast enhancement, and radiomics based on multiparametric MRI was not included. In our study, age, NLR and RDW were selected to evaluate the grade and proliferation potency in glioma patients. The combination of these three clinical factors was associated with the grade (AUCs for differentiating between LGGs and HGGs of 0.7 and 0.82 in the training and validation cohort, respectively; AUCs for differentiating between grade III and grade IV gliomas of 0.65 and 0.60 in the training and validation cohort, respectively) and proliferation potency (AUCs of 0.67 and 0.72 in the training and validation cohort, respectively). Nevertheless, the performance was significantly weaker than that of the radiomics score.

This study has several limitations. First, this is a retrospective evaluation with the data collected from a single center. Multicenter studies with greater sample sizes are needed. Second, the advanced MRI sequences (such as DWI, DTI or perfusion imaging) were not used in this study and need to be added in the future. Third, the 2016 WHO classification includes molecular characteristics such as IDH mutation and 1p/19q codeletion, but these factors were not taken into account in our study. Therefore, molecular markers should be considered in future studies. Fourth, the sample size was relatively limited, and only 39 patients had grade III gliomas. Therefore, the calibration in the validation cohort was not optimal. Finally, the prognostic role of the radiomics score associated with inflammation markers was not assessed and needs to be validated in the future.

In conclusion, multiparametric MRIbased radiomics and peripheral inflammatory markers (age, NLR, and RDW) can be used to assess the grade and proliferation potency accurately for gliomas preoperatively and noninvasively. Such a method is valuable in designing personalized treatment strategies.

## **Conflict of interest disclosure**

The authors declared no conflicts of interest.

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Supplementary Table 1. Characteristics of LGGs and HGGs patients in the training and validation cohorts								
	٦	Training cohort (n=107)		V	Validation cohort (n=45)			
	LGGs	HGGs	p	LGGs	HGGs	p		
Number	36	71	-	11	34	-		
Age								
Mean±SD	44.53±11.31	51.93±22.68	0.001	40.18±8.85	56.79±12.27	<0.001		
NLR								
Median (Q1, Q3)	2.07 (1.72, 3.21)	2.73 (1.97, 4.64)	0.036	1.83 (1.47, 2.89)	3.21 (2.28, 5.12)	0.016		
RDW								
Mean±SD	13.1±1.04	13.36±1.34	0.161	13.21±1.38	13.24±0.82	0.283		
p < 0.05. NLR, neutrophil-lymphocyte ratio; RDW, red cell distribution width; LGGs, low-grade gliomas; HGGs, high-grade gliomas.								

## Supplementary Table 2. Characteristics of Grade III and IV patients in the training and validation cohorts

		Training cohort (n=74)		Validation cohort (n=31)			
	Grade III	Grade IV	р	Grade III	Grade IV	р	
Number	28	46	-	11	20		
Age							
Mean±SD	50.18±13.30	54.72±12.44	0.099	51.27±13.52	26.6±13.25	0.082	
NLR							
Median (Q1, Q3)	3.04 (2.18, 4.63)	2.8 (2.07, 4.72)	0.608	2.25 (2.18, 2.6)	3.20 (2.35, 6.42)	0.043	
RDW							
Mean±SD	13.18±1.05	13.26±0.92	0.448	13.28±0.71	13.69±1.94	0.885	
<i>p</i> < 0.05.		Parente and a second data					

NLR, neutrophil-lymphocyte ratio; RDW, red cell distribution width.

Supplementary Table 3. Characteristics of low Ki-67 and high Ki-67 patients in the training and validation cohorts								
	Т	raining cohort (n=107)		V	Validation cohort (n=45)			
	Low Ki-67 LI	High Ki-67 LI	p	Low Ki-67 LI	High Ki-67 Ll	р		
Number	42	65	-	14	31	-		
Age								
Mean±SD	46.4±12.42	51.6±12.48	0.018	42.86±9.65	57.19±12.73	0.001		
NLR								
Median (Q1, Q3)	2.22 (1.75, 3.48)	2.51 (2.07, 4.53)	0.127	2.2 (2.34, 5.4)	3.42 (2.34, 5.4)	0.013		
RDW								
Mean±SD	13.01±0.84	13.44±13.0	0.116	13.17±1.24	13.26±0.84	0.233		
p < 0.05. NLR, neutrophil-lymphocyte ratio; RDW, red cell distribution width; Ki-67 Ll, Ki-67 labeling index.								



Supplementary Figure. a-f. Compared with the individual sequences, the ROC curves showed the effectiveness of the multiparametric MRI in differentiating between LGGs and HGGs, grade III and grade IV gliomas, and low Ki-67 and high Ki-67 in the training cohort (a-c) and validation cohort (d-f), respectively.